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<p>(54) Title: TIME-CONTROLLED HEARING AID</p> <p>The diagram illustrates the internal architecture of a hearing aid. It features a central processing unit (CPU) connected to various memory units: DATA RAM, PROGRAM-ROM, and PROGRAM-RAM. A digital-to-analog converter (DAC) is connected to the CPU and a sound transducer (2a). Two microphone inputs (2b) feed into an analog-to-digital converter (ADC). The ADC's output is processed by an audio processing and adaptation circuit (6). The circuit also receives signals from a counter (13) and a non-volatile storage unit (14). The counter (13) is connected to the CPU and the non-volatile storage unit (14). The non-volatile storage unit (14) is connected to the CPU and an interface (INTERFACE). The interface is connected to a power source (PS). A sound generator (12) is also connected to the CPU. The final output goes through a power amplifier (PA) and a speaker (3).</p>			
<p>(57) Abstract</p> <p>A hearing aid (1) which comprises a sound transducer (2a, 2b), an analogue-digital converter (3), a digital processing and adaptation circuit (6) for the processing of digital signals, corresponding to audio signals which are received by the transducer (2a, 2b), storage units for the storage of data and programmes for the digital processing and adaptation circuit, a digital-analogue converter (12) and a sound generator (13). The hearing aid also contains a counter, which registers the time for which the hearing aid has been in use, and a non-volatile storage unit (14) in which the utilisation time is summed up. The hearing aid is arranged in such a manner that a comparison is made between the contents of that part of the non-volatile storage unit in which the summed-up utilisation time is stored and one or more limit values, and so that when one or more of the limit values is reached, a special function is initiated.</p>			

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TIME-CONTROLLED HEARING AID

The invention concerns a hearing aid of the kind which comprises a sound transducer, an analogue-digital converter, a digital processing and adjustment circuit for the processing of digital signals, corresponding to audio signals which are received by the transducer, memory units for the storage of data and programmes for the digital processing and adjustment circuit, a digital-analogue converter and a speaker.

10 A hearing aid of this known kind is described, for example, in the United States patent publication no. 4,972,487, which concerns a programmable hearing aid, which also contains data logging means. With this data logger it can be registered how many times each programme is activated, and for how long each programme is used. By the reading out of the data registered, an audiologist or a fitter or the like can ascertain for how long and how many times the individual user of the hearing aid has used the individual programmes over an elapsed period of time.

20 Known hearing aids of this kind are normally sold to the user as a one-time service at a relatively high purchase price. In addition to the hearing aid itself, this purchase price also covers an obligation, which the hearing aid dealer undertakes, to provide the user with service with regard to subsequent adjustment, advice, maintenance etc. for a subsequent period, which is normally of 3 – 5 years. All repairs are covered by a guarantee of 25 1 – 2 years, which thereafter are paid for by the user, but these repairs can, however, be covered if extra insurance is taken out.

30 For several various reasons, it would be desirable if the hearing aids could be sold in connection with subscription arrangements in the same way as e.g. is known in connection with contact lenses, where a start fee is paid

upon establishing a subscription agreement, after which regular subscription fees are paid which cover, e.g. an annual check-up of the eyesight and continuous deliveries of new lenses.

- 5 For the hearing aid dealer, such an arrangement would have the advantage that this would provide a continuous income. For the users of the hearing aids, the advantage would be that the relatively high one-time service price upon acquiring the hearing aid would be spread over a series of years, and the users will also have the advantage that providing the
10 regular subscription fee is paid, they will be ensured that repairs, service etc. of the hearing aid will be carried out and, moreover, that they will be able to have their hearing checked regularly in connection with the subscription.
- 15 However, such a subscription arrangement in connection with hearing aids requires that it is possible to stop the current services if the user does not pay the subscription fees, in the same way as the regular deliveries of new contact lenses can be stopped in connection with lens subscribers.
- 20 This is achieved in a hearing aid of the kind disclosed in the introduction which contains a counter element for the registration of the utilisation time and a storage unit for the storage of this data, and which is characteristic in that the counter element comprises a counter for the registration of the time the hearing aid has been used, that the storage unit for the storage of
25 this data comprises a non-volatile memory in which the utilisation time is summed up, that the hearing aid is arranged in such a manner that a comparison is made between the contents of that part of the non-volatile memory in which the summed-up utilisation time is stored and one or more limit values, and that when one or more of the limit values is reached, a
30 special function is initiated.

The total time for which the hearing aid is used will hereby be registered currently in the hearing aid, and when one or more limit values are exceeded, in that a limit value can be set e.g. for a subscription period, said limit values having been previously stored in the hearing aid, a special 5 function will be initiated which indicates to the user that the subscription period has expired or is nearing expiry. The user can hereafter take the steps necessary for extending the subscription.

As disclosed in claim 2, it can be expedient for the special function which is 10 initiated to consist of a deactivation of the hearing aid, in that e.g. when the limit value is exceeded, a disconnection of the hearing aid battery or other vital functions in the aid can be effected.

As characterized in claim 3, the special function can consist of an alarm 15 arrangement, whereby in the event of a first limit value being exceeded, the user is made aware that the subscription period has expired or is nearing expiry, e.g. by the hearing aid emitting a short acoustic signal which is possibly repeated. If the subscription is not renewed, this can be combined with the deactivation of the hearing aid after a second limit value is 20 exceeded.

Finally, as disclosed in claim 4, the exceeding of a limit value can initiate a changing of the parameters and/or programmes which have influence on the operation of the hearing aid, so that an updating of the function of the 25 hearing aid can take place automatically after a certain period of time, either in connection with the expiration of a subscription period or at a random time determined by the dealer or the audiologist.

The renewal of the subscription can naturally take place by the user paying 30 a visit to the dealer (audiologist), who will update the hearing aid by means

of the PC equipment, which is normally used when the hearing aid is set for use. As disclosed in claim 5, it can be expedient for this to be carried out when the hearing aid is arranged to detect special reactivation signals. The detection of such reactivation signals, which e.g. can be, coded signals, results in the updating of the hearing aid.

As disclosed in claim 6, this updating can, for example, consist of the counter for the summed-up utilisation time being set to zero, so that a new subscription period can be started, or as disclosed in claim 7, that the stored limit value or values are increased corresponding to a new subscription period. With the latter method, the further advantage is achieved that the time counter will thus always contain a measure of the total utilisation time.

Moreover, with the updating, it can be expedient for further changes to be made in the data and/or the programmes which are stored in the hearing aid, as disclosed in claim 8, whereby an automatic updating of the function of the hearing aid is effected. For example, this can be the case in connection with new users, where use is made of a habituation system.

With such a habituation system, there will occur a gradual transition from no hearing aid to full compensation for the user's loss of hearing.

For the user, however, it will be an inconvenience to have to visit the dealer/audiologist to have the hearing aid updated by means of the PC equipment, which the dealer uses for adjustment of the hearing aid.

As disclosed in claim 9, the hearing aid can therefore be supplied with reactivation signals by special audio signals being sent to the hearing aid's microphone. For example, this can be effected by the user telephoning to the dealer/audiologist, or vice-versa, (for example when the subscription

fee for the following period has been paid), and that the audiologist then transfers the code signals via the telephone connection while the user holds the hearing aid close to the telephone receiver. The updating can hereby be effected quickly without the user having to visit the
5 dealer/audiologist.

Other methods by which audio signals can be transferred to the hearing aid can be envisaged. For example, the dealer/audiologist can send a postcard with an audio chip or a tape on which the coded audio signals
10 have been recorded, or use can be made of the Internet to transfer audio signals to the user's hearing aid. After a subscription fee has been paid, the user can thus get the coded signals transferred by calling an Internet address from a PC. The payment of the subscription fee can also possibly be made over the Internet, so that with a single call the user cannot only
15 make the payment but also get the coded signals transferred to the hearing aid.

In connection with the use of coded audio signals as reactivation signals, use can be made, for example, of the DTMF signals (Dual Tone Multi-Frequency), for example well known from the telephone systems, where two simultaneous pure tones are used to signal a digit between 0 and 9. Such signals are relatively easy to detect in the hearing aid's digital signal processing circuit, and at the same time an ordinary telephone keypad can be used as coding apparatus.
20

Finally, as disclosed in claim 10, the hearing aid can be arranged with a number of code keys, pushbuttons or the like, so that the reactivation signals can be entered by the user. This has the advantage that the code can be sent to the user in writing, expressed as the entries, which must be
25

made, after which the user himself can key in the code at a convenient time.

In both cases it will be an advantage that the code is changed from time to
5 time, so that the user cannot just copy a code from a previous subscription period, e.g. by recording the coded audio signals on tape, and use this for the subsequent subscription period(s).

In the following, the invention will be explained in more detail with
10 reference to the drawing, where

fig. 1 shows a block diagram of a digital hearing aid according to the invention, and

15 fig. 2 shows an example of a signal-processing block in a digital hearing aid according to the invention.

An example of a digital hearing aid according to the invention is shown in block diagram form in fig. 1. The hearing aid, which is indicated in general
20 by the reference figure 1, contains one or more sound transducers 2 such as microphones and tele-coils. In the example shown, use is thus made of two microphones 2a and a tele-coil 2b. The analogue signal(s) from the sound transducers 2a and 2b are coupled to an analogue-digital conversion circuit 3, which contains an analogue-digital converter 4 for
25 each of the transducers 2a and 2b.

The digital signal outputs from the analogue-digital converters 4 are coupled to a common digital conduction bus 5, which feeds the signals to a digital signal processing and adaptation circuit 6. This circuit which, for
30 example, can be in the form of a digital signal processor (DSP), and which

will be described in more detail later, is programmed to carry out the necessary operations on the digital signals with the object of effecting the necessary adaptation of the signals and to adjust the hearing aid for the actual user.

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From the digital conduction bus 5, output signals are fed to a digital-analogue converter 12, from which analogue output signals are fed to a sound transducer 13 such as a speaker.

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Furthermore, the hearing aid contains an external memory 14 in relation to the digital signal processing and adaptation circuit 6, which in the example shown is an EEPROM (Electronically Erasable Programmable Read-Only Memory). This external memory 14, which is connected to the digital conduction bus 5, can be provided with programmes, data, parameters etc. that can be entered from a PC 16 via an interface 15. For example, this will be the case when a new hearing aid is allotted to a concrete user, and the hearing aid is adjusted to suit precisely this user, or when a user gets his/her hearing aid updated and/or adjusted by an audiologist for the user's actual loss of hearing.

15

The digital signal processing and adaptation circuit 6, which in the example shown consists of a digital signal processor (DSP), contains a central processor (CPU) 7 and a number of internal storage units 8 - 11, said internal storage units containing data and software which are currently implemented in the digital signal processing and adaptation circuit 6. The circuit 6 thus contains a programme-ROM (Read-Only Memory) 8, a data-ROM 9, a programme-RAM (Random Access Memory) 10 and a data-RAM 11. The two first-mentioned contain programmes and data which constitute permanent elements in the circuit, while the two last-mentioned contain programmes and data which can be replaced or overwritten.

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- The external EEPROM 14 is normally considerably larger, e.g. 4 – 8 times larger, than the internal RAM, which means that certain data and programmes can be stored in the EEPROM for reading into the internal RAMs for execution when there is need for them, in that these special data and programmes can later again be overwritten by the normal operational data and operating programmes. The external EEPROM can thus contain a number of programmes, which are used only in special cases, such as e.g. start-up programmes.
- 10 In the digital signal processing and adaptation circuit 6, the signal processing will be effected in blocks, each of which contains a number of signal processing stages and data operations. These stages will be executed one by one and will be repeated in the individual blocks in the same pattern in fixed time frames. This is illustrated in fig. 2, which shows 15 a single signal-processing block in a temporal sequence, which sequence is repeated during the whole of the hearing aid's operating period.
- The signal processing starts by a Fourier transformation of the signals from the time domain to the frequency domain being carried out on the sampled 20 digital signals from the analogue-digital conversion circuit 3. In the example, use is made of a Fast-Fourier-Transformation (FFT), as illustrated at the stage 20. Hereafter, a compression (COMP) is typically carried out as illustrated at stage 21, with the object of bringing the signals within a desirable processing range. The object of this compression is to 25 adapt the signal to the actual user, in that those frequencies at which the user has a loss of hearing will be raised in relation to the remaining frequencies in such proportion that the hearing loss will be neutralised. There is then effected a filtration by means of an adaptive filter (DFS) at stage 22, the object being to suppress a possible tendency towards 30 acoustic feedback. Moreover, other types of desirable signal processing

will be able to be effected before the last stage 26 in the block, where an inverse Fast-Fourier-Transformation (IFFT) of the signals back to the time domain is carried out. As shown in fig. 1, these signals will be fed to the digital-analogue converter 12, after which the corresponding analogue signals are fed to the speaker 13.

The block described above consisting of a group of stages will, for example, have a temporal sequence which extends over 4 ms, so that the block will be repeated every 4 ms. If, for example, the sampling frequency is 16 kHz, during the course of 4 ms there will be collected 128 samples which are stored in the data-RAM 11. The block oriented signal processing will thus be carried out on such a group of 128 samples, starting with a Fast-Fourier-Transformation in stage 20.

In addition to the already described examples of types of signal processing, the block in fig. 2 will further comprise three system operations or programmes, which are repeated every fourth millisecond.

The object of the programme 23 (Reg. Time) is to register the utilisation time for the hearing aid, and it functions by use of two storage units ("counter" and "hour counter") in data-RAM 11. When the programme 23 is executed, it will read the contents of the storage unit "counter" and increase the value by 1. With a run-through time for a block of 4 ms, an hour will have elapsed when the contents of the storage unit "counter" has reached up to the value 900,000. When this happens, the programme 23 will cause the storage unit "counter" to be set to zero, and the "hour counter" storage unit to be increased by 1. At the same time, the programme will ensure that the new value of the storage unit "hour counter" is transferred to a corresponding storage unit (hour counter) in the external EEPROM 14. The actual number of hours for which the hearing

aid has been in operation will thus always be able to be read out from the external memory 14.

- 5 The programme 24 (Prog. change check) serves to check whether a change should be made to another programme, e.g. if the "hour counter" storage unit has reached one of the stored limit values, or if the user by the activation of an external pushbutton causes an interrupt with the view to changing between two or more conditions or programmes.
- 10 The object of the Programme 25 (Check DTMF) is to test whether the data which is currently being handled in the block contains signals which will give rise to the implementation of an updating of the hearing aid, such as e.g. a zero-setting of the "hour counter" storage unit in the internal data-RAM 11 and in the external EEPROM 14, or an updating of the limit values 15 which are stored in the external EEPROM 14, and possibly a changing of other data in the data-RAM 11, the program-RAM 10 and/or the external EEPROM 14. These signals, which in the following are referred to as reactivation signals, can be any form of coded signals which can be recognized during data processing by the programme 25.
- 20 For example, use can be made of the well-known DTMF signals (Dual Tone Multi-Frequency), where two simultaneous pure tones are used to signal a given digit between 0 and 9. In an FFT-based structure as that described above, it is relatively simple to test whether there are DTMF signals in those signals, which are fed into the digital signal processing and adaptation circuit 6 from the microphones 2. The programme 25 can thus detect such DTMF signals and, providing a given combination is detected, can activate a special programme stored in the external EEPROM 14. The special programme can, for example, reset to zero the 25 "hour counter" storage unit in the internal data-RAM 11 and in the external 30

EEPROM 14 and/or set a new maximum value for the utilisation time, which maximum value can be stored in the external EEPROM 14. Finally, by transferring changes from the external EEPROM 14 to data-RAM 11 and program-RAM 10, the special programme can carry out an updating or
5 changing of the data and/or programmes for the digital signal processing.

The reactivation signals, such as e.g. DTMF signals, can be introduced in the signals from the sound transducers, e.g. by the supply of audio signals to the microphones 2, or by signals which are generated by means of a
10 code keypad in the hearing aid being introduced into the hearing aid's signal circuit. Finally, the reactivation signals can naturally be fed directly to the hearing aid, e.g. by an audiologist using a PC 16 and an interface 15, such as shown in fig. 1. However, this naturally requires that the
15 hearing aid user visits the audiologist with his/her hearing aid, or gives the audiologist access to the aid in another manner.

If this involves audio signals which are transferred to the hearing aid's microphones, this can be carried out e.g. over a normal telephone line, in that the hearing aid user can hold the hearing aid up against the telephone
20 handset, so that the microphones in the hearing aid can receive the sound from the telephone receiver. The coded signals can also be transferred to the hearing aid user in other ways, e.g. in the form of tape recordings or audio chips with the desired code sequence which can be sent to the user as ordinary mail.

25 The audio signals can also be transferred to the user's hearing aid via the Internet, in that after the subscription fee has been paid, the user can call an Internet address from his/her PC and have the code signals transferred. The payment of the subscription fee can possibly also take place over the

Internet, so that both the payment and the transfer of the coded signals to the hearing aid can be effected with a single call by the user.

- If a code keypad is used on the hearing aid, in its simplest form this can
5 consist solely of two keys with which the hearing aid users can enter a code sequence, which has been sent to them. More than two keys can, of course, be used for the entering of code sequences, such as e.g. a telephone keypad of the kind normally used.
- 10 In the fitting of a user with a hearing aid, the dealer/audiologist will have provided the hearing aid with the programmes and the data, which are necessary for its operation. There will thus be entered the programmes and data which control the signal adjustment with the view to compensating for the user's hearing loss for at least a first period. Moreover, among other
15 things, at least the maximum utilisation time for the first subscription period will be entered and, if a habituation system is used where the compensation is to be gradually increased, the data and/or the programmes, which are to be used in the signal processing for at least the following period.
- 20 When the hearing aid is switched on by the user and taken into use, the first thing to be entered from the external EEPROM 14 will be a start-up programme which, among other things, checks whether the summed-up utilisation time (stored in the "hour counter" storage unit), has exceeded
25 one or more of the stored limit values for the utilisation time. If this is the case, this will result in the initiation of a special programme which, if a subscription period has expired or is about to expire, can e.g. execute an alarm or signalling function, e.g. in the form of a series of audio signals, and/or which can deactivate the hearing aid e.g. by breaking the

connection to the speaker, after which the normal operating programme will not be initiated.

5 If none of the stored limit values have been exceeded, an operating programme will read in from the external EEPROM, after which the hearing aid will function in the normal manner.

In the updating of the hearing aid, i.e. when the hearing aid detects a series of reactivation signals, a special programme will be initiated in the
10 digital circuit which checks whether the coded signal is that which is expected (i.e. corresponding to a code which is stored in the EEPROM), and in such case among other things an updating of the stored limit values will be effected, e.g. in the form of a writing-up for the expiry of the next subscription period, or alternatively a setting of the summed-up utilisation
15 time to zero. Moreover, e.g. when a habituation system is used, a changing of the parameters and/or programmes which are used for the signal processing will take place, e.g. by the selection from the EEPROM of new data and/or programmes which are to be used in connection with the operating programme. Finally, a new code can possibly be selected for the
20 reactivation signals, and this code will then be that which is expected to be used at the next updating of the hearing aid.

The said limit values for the utilisation time can be determined in different ways. For example, an upper limit value can be entered which corresponds
25 to the lifetime it is desired to give the hearing aid, e.g. 3 years. Such a determination is encumbered with considerable uncertainty, in that the user pattern is not known. Normally, the daily use will be estimated to be 16 hours, so that an upper limit of 3 years will correspond to a summed-up utilisation time of approx. 18,000 hours. After a certain period of time,
30 during a service visit to the dealer/audiologist, the utilisation time can,

however, be read out from the hearing aid to a PC programme, and since the date on which the hearing aid was taken into use is known, this provisional utilisation time can be used to estimate the average daily use with greater precision, so that new limits can then be entered with a greater degree of certainty.

C L A I M S

1. Hearing aid (1) which comprises a sound transducer (2a, 2b), an analogue-digital converter (3), a digital processing and adaptation circuit (6) for the processing of digital signals, corresponding to audio signals which are received by the transducer (2a, 2b), storage units for the storage of data and programmes for the digital processing and adaptation circuit, a digital-analogue converter (12), a sound generator (13), a counter element for the registration of utilisation time, and a storage unit for the storage of utilisation time, *characterized in* that the counter element contains a counter which registers that time for which the hearing aid has been in use, that the storage unit for the storing of the utilisation time comprises a non-volatile memory unit (14) in which the utilisation time is summed up, that the hearing aid is arranged in such a manner that a comparison is made between the contents of that part of the non-volatile memory unit in which the summed-up utilisation time is stored and one or more limit values, and that when one or more of the limit values has been reached, a special function is initiated.
2. Hearing aid according to claim 1, *characterized in* that the special function, which is initiated when a limit value is reached is a deactivation of the hearing aid.
3. Hearing aid according to claim 1 or 2, *characterized in* that the special function which is initiated when a limit value is reached is an alarm function.
4. Hearing aid according to claim 1, 2 or 3, *characterized in* that the special function which is initiated when a limit value is reached is a changing of

parameters and/or programmes which are stored in the digital processing and adaptation circuit (6).

5. Hearing aid according to one or more of the claims 1 – 4, characterized in that the digital adaptation and signal processing circuit (6) is arranged to detect the presence of reactivation signals in the digital signal flow and, depending on the presence of such signals, to initiate one or more special functions.
10. 6. Hearing aid according to claim 5, characterized in that the hearing aid is arranged in such a manner that upon detection of a reactivation signal, a zero-setting is carried out of that part of the non-volatile memory unit in which the utilisation time is summed up.
15. 7. Hearing aid according to claim 5, characterized in that the hearing aid is arranged in such a manner that upon detection of a reactivation signal, there is carried out an increase of one or more of the limit values with which the summed-up utilisation time is compared.
20. 8. Hearing aid according to claim 5, 6 or 7, characterized in that upon detection of a reactivation signal, a changing of parameters and/or programmes is also carried out.
25. 9. Hearing aid according to one or more of the claims 5 – 8, characterized in that the hearing aid is arranged in such a manner that the reactivation signals are introduced into the hearing aid's digital signal flow, this being effected by supplying special audio signals, corresponding to the reactivation signals, to the hearing aid's transducer (2a, 2b).

10. Hearing aid according to one or more of the claims 5 – 8, *characterized in* that the hearing aid is arranged in such a manner that the reactivation signals are introduced into the hearing aid's digital signal flow, in that the hearing aid has a number of code keys with which a special code, 5 corresponding to the reactivation signals, is fed into the hearing aid.

1/2

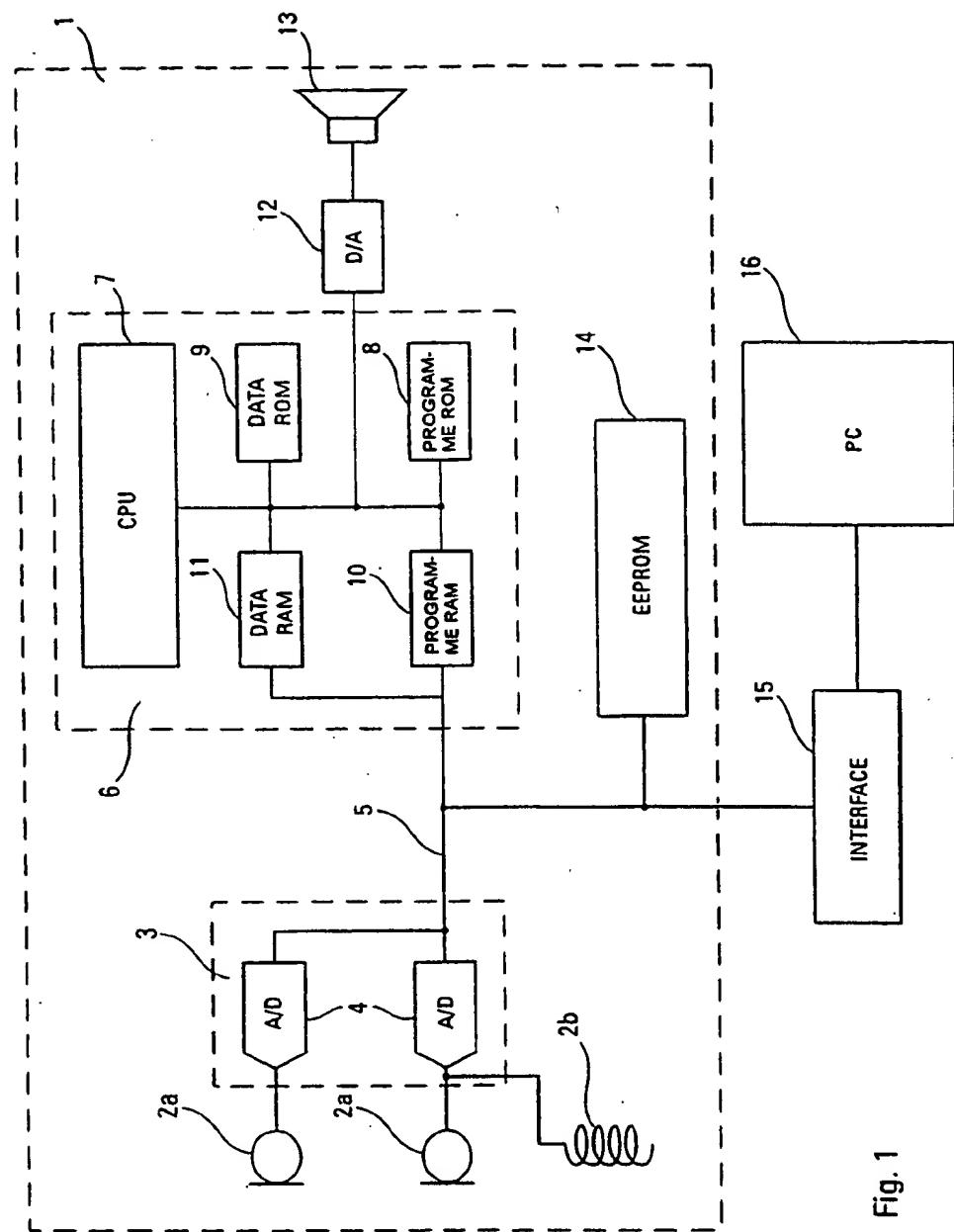


Fig. 1

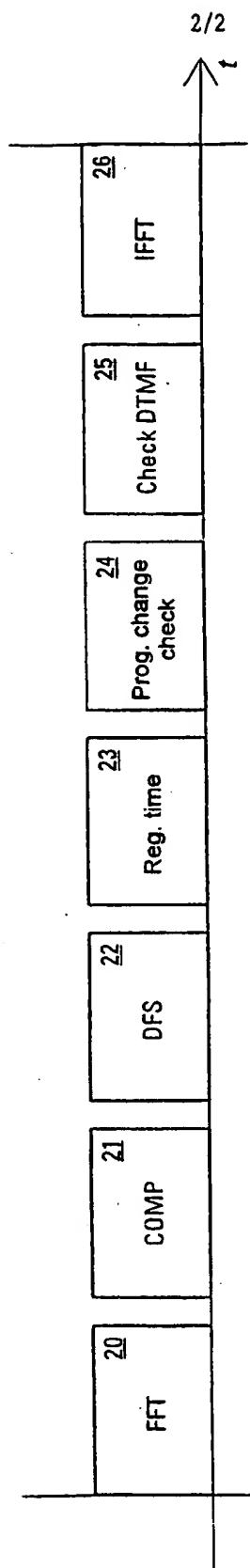


Fig. 2

INTERNATIONAL SEARCH REPORT

International application No.

PCT/DK 99/00687

A. CLASSIFICATION OF SUBJECT MATTER

IPC7: H04R 25/00

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC7: H04R, A61F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

SE,DK,FI,NO classes as above

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 4972487 A (MANGOLD ET AL), 20 November 1990 (20.11.90), column 1, line 37 - line 58, abstract --	1
A	US 5210803 A (MARTIN ET AL), 11 May 1993 (11.05.93), abstract -----	1

 Further documents are listed in the continuation of Box C. See patent family annex.

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Information on patent family members

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